2589-6458/19



A Simple Acoustic Sensor Test Platform for Respiratory and Cardiac Acoustical Monitoring

D. John Doyle^{1,*}

¹Department of General Anesthesiology, Cleveland Clinic Abu Dhabi, Abu Dhabi, United Arab Emirates

Abstract: The properties of various acoustic interfaces (stethoscopes) for respiratory monitoring and phonocardiography are compared using a special-purpose custom-built electronic vibration platform that can be driven by an electronic test signal. Sample sensitivity data for various stethoscope designs are presented in this study.

Keywords: Bio-acoustics, Breath sounds, Phonocardiogram, Stethoscope sensitivity, Respiratory monitoring, Phonocardiography.

| Article History Received: August 19, 2019 | Revised: September 17, 2019 | Accepted: October 09, 2019 |
|---|-----------------------------|----------------------------|
|---|-----------------------------|----------------------------|

1. INTRODUCTION

Since the earliest of times, a need has existed for a simple, dependable means of cardiorespiratory monitoring. In antiquity, respiratory monitoring consisted of careful observation of breathing patterns, focusing especially on rate and rhythm as well as contributions from the diaphragm, thorax (intercostal muscles), and accessory muscles. Similarly, in early times, cardiac monitoring primarily focused on the analysis of the pulse, with later innovations in blood pressure measurement and cardiac auscultation contributing in important ways. In modern medicine, the need for respiratory monitoring has become important with the frequent use of opioids and other respiratory depressants, especially during perioperative care or with critically ill patients [1 - 8]. Given this clear clinical need, the search for simple and dependable methods of patient monitoring has been the focus of numerous researchers, who are looking at acoustical methods of respiratory and cardiac monitoring. To this end, this brief technical report is intended to provide information on building an acoustical test platform of potential value to these investigators.

1.1. Stethoscopes

Precordial stethoscopes and esophageal stethoscopes are often used to listen to breath and heart, especially during surgical anesthesia. Precordial stethoscopes are typically employed on a weighted chest piece or a con-ventional stethoscope head in contact with the chest (Fig. 1), while esophageal stethoscopes are typically soft, thin-walled tubes inserted into the esophagus in the unconscious patient. Esophageal stethoscopes usually feature a distal cuff designed to optimize sound transmission and a male Luer connector for attachment to standard earpieces. Many models support core body temperature measurements as well. Both types of stethoscopes can be very useful in monitoring changes in breath or other bioacoustic phenomena. Examples include the detection of crackles, wheezes and unilateral ventilation resulting from deliberate or inadvertent endob-ronchial intubation.



Fig. (1). Two conventional stethoscope heads (left side), along with a weighted precordial chest piece (upper right) and a stethoscope head from a disposable stethoscope (bottom right). The model on the bottom left is a Littman Classic II SE, while the model on the top left is a generic (unbranded) unit.

^{*} Address correspondence to this author at the Department of General Anesthesiology, Cleveland Clinic Abu Dhabi, Abu Dhabi, United Arab Emirates; E-mail: djdoyle@hotmail.com

112 The Open Anesthesia Journal, 2019, Volume 13

As the science of acoustics progresses, a number of innovations lead to improved stethoscope designs beyond the original 1816 monaural design by René Laennec [9]. For example, important research by Rappaport and Sprague looking at the effects of tubing bore [10] and the quality of the ear fitting [11] lead to innovations in use. In addition to directly listening to breath sounds via an earpiece, further innovations have led to developments, such as the electronic transduction, amplification and transmission of breath sounds, as well as in providing methods for advanced computer-based analysis. However, one important aspect significant to such undertakings is to evaluate various stethoscope assemblies to which a microphone is to be attached. This was the aim of this report.

1.2. Research Platform

While it is relatively easy to calibrate a microphone for use with acoustical respiratory monitoring, it can be somewhat more difficult to compare the effectiveness of various stethoscope assemblies to which a recording microphone is to be attached. As noted, precordial stethoscope assemblies usually come in two forms, the first in the form of a weighted chest piece and the second in the form of a conventional stethoscope head (Fig. 1). In either case, a miniature microphone as shown in the bottom of Fig. (2) is attached to the stethoscope assembly through a short piece of tubing. The question then naturally arises, as to which stethoscope best transfers the vibrations of the connected microphone? This issue was addressed by developing a special test platform for this purpose.

As shown in Figs. (2 and 3) the test platform consists of a small loudspeaker coupled to a plastic vibration test surface and driven by an audio amplifier (located at the bottom right of Fig. 2), this amplifier, in turn, is driven by a signal source such as a function generator. Additionally, the relative sound intensity obtained at the stethoscope under test was measured using a RadioShack 33-3013 miniature omnidirectional electret microphone connected to the stethoscope head through a short piece of tubing and amplified using a second audio amplifier, a RadioShack miniature audio amplifier (Catalog # 2771008) was displayed on a USB oscilloscope (Picoscope 2205).

Table 1 shows the obtained results with a 1000 Hz test signal. Strikingy, there was an approximately 6-fold variation in the sensitivity of the various stethoscope assemblies when tested with a 1000 Hz sinusoid, with the diaphragm of the Littman Classic II SE being the most sensitive (relative sensitivity 1.0) and the bell of the generic model tested type being the least (relative sensitivity 0.16). It is worth noting that different results might be obtained with different stimulus frequencies or conditions where the assembly under test is made to contact the test surface more firmly, for example, using a weight placed on the unit.

2. IDEAS FOR FUTURE WORK

As the objective of this short communication was to introduce the readers of the journal to a simple acoustical test platform that may be of value to investigators, rather than to comparatively evaluate a variety of stethoscopes, the present study investigated the sensitivity of only a limited number of stethoscopes, and only at a single test frequency (1000 Hz). It is hoped, however, that this report will encourage future studies following the footsteps of this initiative.



Fig. (2). The test platform used to compare the various stethoscope assemblies. The platform consists of a small loudspeaker coupled to a plastic vibration test surface (light blue color) and driven by an audio amplifier, the amplifier in turn being driven by a signal source such as a function generator (upper left). The signal generator used is an inexpensive DDS (direct digital synthesis) model FG-100 readily available on eBay and operating in sinusoidal waveform mode at 1000 Hz. A RadioShack 33-3013 miniature omnidirectional electret microphone is connected to the stethoscope head under test through a short piece of tubing and amplified using a RadioShack miniature audio amplifier (Catalog # 2771008) for display on a USB oscilloscope (upper left). Table 1 shows the obtained results with a 1000 Hz test signal. Note that the system used two audio amplifiers, the first (located at the bottom right of Fig. 2) to drive the loudspeaker and the second (the RadioShack amplifier) to amplify the microphone signal for presentation to the USB oscilloscope.

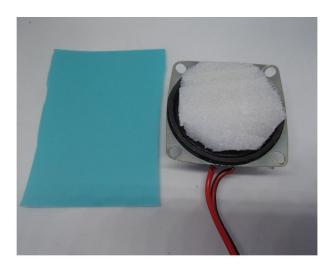


Fig. (3). Photograph illustrating some construction details for the vibration test platform shown in Fig. (2). The loudspeaker is glued to the plastic sheet shown on the left, with the white coupling material used to ensure a good acoustic interface.

Possible future studies based on the described platform that might be of interest include testing of additional stethoscopes in common use, examining the effect of the degree to which the assembly under test is made to contact the test surface, and (especially) examining the results obtained at frequencies other than 1000 Hz. In the case of the last suggestion, it would be possible to measure the results over a specific range of frequencies using a more advanced setup known as sweep frequency response testing. In such an arrangement, the test signal is made to vary over a range of frequencies (*e.g.*, 50 Hz to 5000 Hz) while the response to the varying test signal is simultaneously recorded using a specialized test apparatus. The result is a frequency response plot (Bode plot), providing a quantitative measure of the spectral characteristics of the system.

Table 1. Relative peak-to-peak amplitude of the 1000 Hz signal obtained for four stethoscope assemblies (Fig. 1), scaled relative to the diaphragm side of the Littman Classic II SE unit (reference unit). The absolute sound intensity at the vibration plate was measured at 79.1 dB SPL (Aweighted) using an EXTECH Model 407750 Digital Sound Level Meter, while the relative sound intensity obtained at the stethoscope under test was measured using a RadioShack 33-3013 miniature omnidirectional electret microphone connected to the stethoscope head through a short piece of tubing and amplified using a RadioShack miniature audio amplifier (Catalog # 2771008) for display on a USB oscilloscope (Picoscope 2205). All assemblies were placed on the test surface and held in position by their weight except the disposable unit (test assembly 5), which on account of its lightweight had to be secured with a double-sided adhesive disk specifically designed for the use of stethoscope (3M Model 2181).

| Stethoscope Assembly Under Test | Figure Reference | Voltage Ratio |
|---|--------------------------|-----------------|
| Test assembly 1 Littman Classic II SE – diaphragm side | Figure 1 Bottom left | 1.0 (reference) |
| Test assembly 2 Littman Classic II SE – bell side | Figure 1 Bottom left | 0.55 |
| Test assembly 3 Generic stethoscope – diaphragm side | Figure 1 Upper left | 0.79 |
| Test assembly 4 Generic stethoscope – bell side | Figure 1 Upper left | 0.16 |
| Test assembly 5 Diaphragm only disposable stethoscope | Figure 1 Bottom right | 0.25 |
| Test assembly 6 Weighted chest piece | Figure 1 Upper right | 0.24 |

CONCLUSION

Although a variety of methods are available for the assessment of patient breathing, bio-acoustical methods of

respiratory assessment offer some special advantages. To this end, various acoustic interface designs were compared using a special-purpose custom-built electronic vibration platform driven by an electronic test signal. It was found that there was an approximately 6-fold variation in the sensitivity of the various stethoscope assemblies when tested with a 1000 Hz sinusoid, with the diaphragm of the Littman Classic II SE being the most sensitive (relative sensitivity 1.0) and the bell of the generic model tested type being the least (relative sensitivity 0.16).

CONSENT FOR PUBLICATION

Not applicable.

FUNDING

None.

CONFLICT OF INTEREST

The author declares no conflict of interest, financial or otherwise.

ACKNOWLEDGEMENTS

Declared none.

REFERENCES

- Pinsky MR, Clermont G, Hravnak M. Predicting cardiorespiratory instability. Crit Care 2016; 20: 70.
- [http://dx.doi.org/10.1186/s13054-016-1223-7] [PMID: 26984263]
 [2] Di Fiore JM. Neonatal cardiorespiratory monitoring techniques. Semin Neonatol 2004; 9(3): 195-203.
- [http://dx.doi.org/10.1016/j.siny.2003.11.009] [PMID: 15050212]
- Buhre W, Rossaint R. Perioperative management and monitoring in anaesthesia. Lancet 2003; 362(9398): 1839-46.
 [http://dx.doi.org/10.1016/S0140-6736(03)14905-7] [PMID: 146543 24]
- [4] Hunt CE. Cardiorespiratory monitoring. Clin Perinatol 1991; 18(3): 473-95.
- [http://dx.doi.org/10.1016/S0095-5108(18)30508-6] [PMID: 1934852]
 [5] Sackner MA. Non-invasive cardiorespiratory monitoring during sleep.
- Eur Respir J Suppl 1990; 11: 545s-6s. [PMID: 2278626]
- [6] Waxman K. Invasive cardiorespiratory monitoring. Emerg Med Clin North Am 1986; 4(4): 775-89.
 [PMID: 3536439]
- [7] Abraham E. Noninvasive monitoring of cardiorespiratory parameters. Emerg Med Clin North Am 1986; 4(4): 791-807.
 [PMID: 3096689]
- [8] Hodgman JE, Cabal LA. Cardiorespiratory monitoring in the high-risk infant. Acute Care 1986; 12(3-4): 165-94.
 [PMID: 3333714]
- [9] Roguin A. Rene theophile hyacinthe laënnec (1781-1826): The man behind the stethoscope. Clin Med Res 2006; 4(3): 230-5. [http://dx.doi.org/10.3121/cmr.4.3.230] [PMID: 17048358]
- [10] Rappaport MB, Sprague HB. The effects of tubing bore on stethoscope efficiency. Am Heart J 1951; 42(4): 605-9.
- [http://dx.doi.org/10.1016/0002-8703(51)90156-1] [PMID: 14877754]
 [11] Rappaport MB, Sprague HB. The effects of improper fitting of stethoscope to ears on auscultatory efficiency. Am Heart J 1952; 43(5): 713-5.

[http://dx.doi.org/10.1016/0002-8703(52)90046-X] [PMID: 14923613]

© 2019 D. John Doyle.

This is an open access article distributed under the terms of the Creative Commons Attribution 4.0 International Public License (CC-BY 4.0), a copy of which is available at: (https://creativecommons.org/licenses/by/4.0/legalcode). This license permits unrestricted use, distribution, and reproduction in any medium, provided the original author and source are credited.